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the software is designed as a teaching and demonstration aid, and is available via the website <http://www.gemssoftware.org/>. there are a number of pre-recorded electrogram examples available for different patient types, which can be downloaded from the website. following a single demonstration, the software is free for use by all academic users. the software is not limited to single electrode recordings, and can import a range of data sources, including extracardiac data, even for multiple electrodes on a single catheter. for example, we have recorded pericardial effusions from both the left and right chest using a dual-site suction catheter system for more than 24-hours in canine models of cardiac dysrhythmias [10]. we have recorded primary human right atrial fibrillation and flutter [11] and fast atrial tachycardia at the base of the left atrium, as well as slow atrial tachycardia (approximately 170 bpm) at the apex of the atrium in patients with coronary disease [12]. we have also shown gems can record, analyze, and simulate left atrial signals recorded using a transesophageal echocardiographic probe in patients undergoing electrophysiological study [13]. the input to the analysis routines in gems are time-series of raw data from the electrode array, known as time traces. each of these traces corresponds to a single channel of the array. (the time trace data for the electrodes near the surface of the stomach are also processed, however, so that three-dimensional interpretations of activation propagation are possible.) these data are typically stored as time-series data with a specific time resolution and spike-based interface, as such, the output of gems is a set of data in a standard format for most common technical computing packages, and thus analysis can proceed using traditional technical computing methods [12]. the data format of gems is saved using a unique identifier for each electrode in the array, such that the raw electrode data can be extracted, stored, or re-imported at a later date. this allows for time-course analysis of electrical propagation to be performed on datasets which were not initially acquired by gems. the raw electrode data is stored, by default, with a data format suitable for traditional technical computing packages (such as matlab or spm), but for users with a programming background, the data can be saved in a standard format for commonly used file-based data processing packages, such as the free open-source file format hdf5 (the hierarchical data format).

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importing and applying the model (according to the instructions in the help file) requires the specification of five key parameters for gems: the start and end of the recording period, the time resolution of the tfr (number of data points per recording period), the duration of the recording period, the number of events per second of data, and the number of channels to be processed. these parameters may be adjusted to optimize the visualization parameters (for example, number of events per time resolution, resolution of the color, number of channels to be displayed, number of channels for display), to help the user choose appropriate settings and to generate visualizations that are comparable and interpretable across participants and experiments, we have defined matlab scripts to calculate the model parameters from the fields and files described in the sections above. these scripts have been implemented in two different versions. one version processes data from whole-head eeg recordings and applies the model to all channels simultaneously, while the other version processes the same data, but allows the user to select groups of channels for the visualizations of the electrophysiological activity (processing mode: full or groupwise). the first section describes the problem of identifying the activity of interest from non-brain sources, particularly, if heart rate variability (hrv) and muscle artifacts are present in the data, then the model has to incorporate a model of these nuisance components. it has previously been demonstrated that the temporal heart rate variability is influenced by the cognitive state of a subject [5, 26], and that the spectral power of hrv is affected by cognitive performance. in our experiments, in order to identify the activity of interest, hrv and muscle artifacts were estimated from all eeg channels and the results were subtracted from the brain activity of interest. we then used regression to estimate the strength of the interaction between brain activity and hrv, which can be applied to the brain activity of interest. spectral, autoregressive and time-frequency decomposition methods are used in this study to understand which components contribute to the hrv. once the hrv is modeled, the approach is to attribute the variance of the hrv to that of the true brain activity. an autoregressive model [29] was used to model the hrv signals. the ar models were parameterized using least-squares or orthogonal estimation (via the arest function in matlab) and implemented in a way that enables measurement of a phase shift and the power of the estimated ar model for each frequency. muscle artifacts and spatial noise were estimated using the band-passed spatial filters described in borbatzadeh et al. [25]. the eeg data can be visualized with a single scalar tfr that shows the distribution of time periods in which the specified channels were active (either with events or spiking activities in the specified time interval) at a desired spatial resolution. 5ec8ef588b

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